Rationale and Objectives: To evaluate the correlations of tracheal volume and collapsibility on inspiratory and end-expiratory computed tomography (CT) with lung volume and with lung function in smokers.

Materials and Methods: The institutional review board approved this study at each institution. 85 smokers (mean age 68, range 45–87 years; 40 females and 45 males) underwent pulmonary function tests and chest CT at full inspiration and end-expiration. On both scans, intrathoracic tracheal volume and lung volume were measured. Collapsibility of the trachea and the lung was expressed as expiratory/inspiratory (E/I) ratios of these volumes. Correlations of the tracheal measurements with the lung measurements and with lung function were evaluated by the linear regression analysis.

Results: Tracheal volume showed moderate or strong, positive correlations with lung volume on both inspiratory \( r = 0.661, P < .0001 \) and end-expiratory \( r = 0.749, P < .0001 \) scans. The E/I ratio of tracheal volume showed a strong, positive correlation with the E/I ratio of lung volume \( r = 0.711, P < .0001 \). A weak, negative correlation was found between the E/I ratio of tracheal volume and the ratio of forced expiratory volume in the first second to forced vital capacity \( r = -0.436, P < .0001 \). Also, a weak, positive correlation was observed between the E/I ratio of tracheal volume and the ratio of residual volume to total lung capacity \( r = 0.253, P = .02 \).

Conclusions: Tracheal volume and collapsibility, measured by inspiratory and end-expiratory CT scans, is related to lung volume and collapsibility. The highly collapsed trachea on end-expiratory CT does not indicate more severe airflow limitation or air-trapping in smokers.

Key Words: Tracheal volume; lung volume; chronic obstructive pulmonary disease; tracheomalacia.

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between inspiratory and expiratory scans significantly correlated to the changes in MLD. Further, more recent studies have demonstrated significant correlations between MLD and lung volume (LV) \(^{(15,16)}\). Based on these observations, it can be predicted that the observations of Ederle and colleagues would be reproduced using volumetric measurements, such as LV and tracheal volume.

We therefore hypothesized that tracheal volume and changes in tracheal volume on inspiratory and end-expiratory CT scans would be correlated to LV and changes in LV among smokers. Although CT-based volumetric analysis of the whole lung has been gradually performed in COPD \(^{(15–19)}\), published information on tracheal volumetric measurements is still limited \(^{(20)}\). With the development of imaging technology, it has become easier to advance the methodology for measuring tracheal size from dimensional to volumetric indices. Furthermore, it would be of interest to evaluate whether or not tracheal volume and collapsibility is correlated with lung function, and whether or not volumetric measurements of the trachea are equivalent to dimensional measurements.

Thus, the aims of this study are: 1) to verify the correlations between tracheal volumetric measures, including tracheal collapsibility, and LV measures on inspiratory and end-expiratory CT scans; 2) to evaluate the relationship between tracheal collapsibility and lung function; and 3) to confirm the correlations between tracheal volumetric measures and dimensional measures.

**MATERIALS AND METHODS**

This retrospective study was approved by the institutional review board at each institution. Informed consent was obtained from all subjects. The subjects’ CT and clinical data used in this study were partially analyzed with a different objective for other research \(^{(15)}\).

**Subjects**

Between March 2005 and February 2008, 184 subjects were enrolled in the Lung Tissue Research Consortium (LTRC), a multicenter trial for pulmonary diseases, at four institutions, including Mayo Clinic at Rochester, University of Michigan, University of Pittsburgh, and University of Colorado. CT scans and patients’ clinical information provided for this study were collected in accordance to the protocols outlined by the LTRC. Further information on the LTRC, including its mission and inclusion criteria, is available on its website (www.ltrcpublic.com). From the 184 subjects, 85, who underwent chest CT with two standardized protocols, were eventually selected and analyzed in this study. Exclusion criteria for this study included: 1) use of different CT scanners that were not selected for this study \(^{(n = 8)}\), 2) CT scans with contrast medium or different slice thickness \(^{(n = 31)}\), 3) different tube current or voltage \(^{(n = 15)}\), 4) no available end-expiratory CT scan \(^{(n = 6)}\), 5) no history of cigarette smoking \(^{(n = 1)}\), 6) previous history of lung resection \(^{(n = 5)}\), 7) severe artifacts on CT images \(^{(n = 4)}\), and 8) presence of pneumothorax, lobar atelectasis, large bullae \((>3\,\text{cm in diameter})\), severe fibrosis, or a mass \((>3\,\text{cm in diameter})\) \(^{(n = 29)}\).

The characteristics of the 85 subjects are summarized in Table 1. Forty females and 45 males were included (mean age 68 years, age range 45–87 years). All subjects were current or former smokers and their mean smoking index was 48.4 pack-years \pm 32.9.

**Pulmonary Function Tests**

All 85 subjects performed prebronchodilator spirometry, including forced expiratory volume in the first second \((\text{FEV}_1)\) and forced vital capacity \((\text{FVC})\), according to American Thoracic Society standards, as described previously \(^{(21)}\). \(\text{FEV}_1\) was also expressed as the percentages of predicted values. Residual volume \((\text{RV})\) and total lung capacity \((\text{TLC})\) were measured by plethysmography \(^{(22)}\). The results of pulmonary function tests \((\text{PFT})\) are summarized in Table 1.

According to the Global Initiative for Chronic Obstructive Lung Disease \((\text{GOLD})\) staging \(^{(23)}\), 85 subjects were classified as follows: smokers with normal lung function, \(n = 14\); GOLD stage 1, \(n = 14\); stage 2, \(n = 38\); stage 3, \(n = 11\); and stage 4, \(n = 8\).

**Thin-section CT**

All subjects were scanned at full inspiration and full expiration \((\text{end-expiration})\), without receiving a contrast medium. Before CT scanning, subjects were coached to hold their breath at full inspiration and full expiration. Among the 85 subjects, 46 subjects were scanned with 16-detector CT \((\text{LightSpeed 16 or LightSpeed Pro16, GE Medical Systems, Milwaukee, WI})\). Images were obtained using 140 kV and 300 mA. Rotation time was 0.53 seconds and the matrix size was 512 × 512 pixels. Images were reconstructed with a 1.25-mm-slice thickness \((\text{with 0.625 mm overlapping})\), using the “Bone” algorithm. The other 39 subjects were scanned with 64-detector CT \((\text{Sensation 64, Siemens Healthcare, Munich, Germany})\). Tube voltage was 140 kV and tube current varied by automatic regulation \((\text{approximately 75–450 mA})\), which was based on the slice location and the subject’s body.

**TABLE 1. Clinical Characteristics of the 85 Subjects**

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Mean ± SD</th>
<th>(Range)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age (y)</td>
<td>67.8 ± 8.0</td>
<td>(45–87)</td>
</tr>
<tr>
<td>Smoking index (pack-years)</td>
<td>48.4 ± 32.9</td>
<td>(2–180)</td>
</tr>
<tr>
<td>FEV(_1)/FVC</td>
<td>0.56 ± 0.14</td>
<td>(0.17–0.83)</td>
</tr>
<tr>
<td>FEV(_1) (%predicted)</td>
<td>60.8 ± 33.6</td>
<td>(14–126)</td>
</tr>
<tr>
<td>RV/TLC</td>
<td>0.50 ± 0.10</td>
<td>(0.32–0.73)</td>
</tr>
<tr>
<td>TLC (L)</td>
<td>6.45 ± 1.34</td>
<td>(4.10–10.20)</td>
</tr>
<tr>
<td>RV (L)</td>
<td>3.24 ± 0.97</td>
<td>(1.50–7.00)</td>
</tr>
</tbody>
</table>

FEV\(_1\), forced expiratory volume in 1 second; FVC, forced vital capacity; RV, residual volume; SD, standard deviation; TLC, total lung capacity.
habitus. Rotation time was 0.5 seconds and the matrix size was 512 × 512 pixels. Images were reconstructed with a 1.0-mm-slice thickness (with 0.5 mm overlapping), using the “B46f” algorithm.

**Measurements of the Trachea**

The cross-sectional area of the trachea and intrathoracic tracheal volume were measured by a thoracic radiologist (T.Y., with 9 years’ experience in interpreting thoracic CT) using open-source software (Image J, National Institutes of Health, Bethesda, MD; [http://rsb.info.nih.gov/ij](http://rsb.info.nih.gov/ij)), without prior knowledge of clinical information. On an axial CT image, the software automatically segmented the lumen of the trachea from the soft tissues in the mediastinum, using thresholds of -1024 and -500 Hounsfield units, which was followed by the measuring of the cross-sectional area of the trachea (Fig 1). To measure the cross-sectional area of the trachea, two anatomic levels were selected on inspiratory scans (1 cm above the aortic arch and 1 cm above the carina), according to the most recent investigation (9). On end-expiratory scans, cross-sectional areas of the trachea were also measured at the same levels, determined by interpreting all anatomical observations. CT images were set with lung window to perform these measurements.

Intrathoracic tracheal volume was also measured using the same software on both inspiratory and end-expiratory scans. In brief, the following process was performed. 1) The radiologist selected all CT images that include the trachea, from the top of the apex to the carina. 2) The software showed the images for every two slices because the original scan had a 50% overlap. 3) Extratracheal air regions (the lungs, bronchi, and esophagus) were automatically segmented by the software and manually excluded on each image. 4) A relatively large measuring area was set in the center of the chest, which included the trachea throughout the selected images. 5) The software measured cross-sectional areas of the trachea on the all selected images. 6) The total cross-sectional area was calculated, and intrathoracic tracheal volume was obtained by multiplying the total cross-sectional area by slice thickness. It took approximately 20 minutes to complete the whole process per subject.

Collapsibility of the tracheal cross-sectional area or tracheal volume was calculated by the expiratory/inspiratory (E/I) ratios of these two indices.

**Measurements of the Lung Volume**

LV was full-automatically measured by different open-source software (Airway Inspector, Brigham and Women’s Hospital, Boston, MA; [www.airwayinspector.org](http://www.airwayinspector.org)), as described previously (15). In brief, the software 1) segmented the lung parenchyma (−1024 to −500 Hounsfield units) from the chest wall and the hilum, 2) created a density histogram of the lung parenchyma, and 3) measured LV by summing all pixels included in the histogram and multiplying them by slice thickness. In each subject, it was confirmed by an operator (T.Y.) that the software properly excluded the trachea and the main bronchi from the measured lung field. The E/I ratios of LV were calculated by the operator.

**Reproducibility of Tracheal Volume Measurements**

Intraobserver error was tested by having one observer (T.Y.) measure tracheal volume twice on inspiratory scans in 20 subjects, who were randomly selected from a total of 85 subjects. The second measurement was performed 2 months after the first session. To evaluate interobserver error, two observers (T.Y., A.D.) independently measured tracheal volume in the 20 subjects. Analysis of intra- and interobserver reproducibility was conducted using the Bland-Altman analysis (24).

**Statistical Analysis**

All statistical analyses were performed using JMP 7.0 software (SAS Institute, Cary, NC). Data were expressed as mean ± standard deviation. The linear regression analysis was used to estimate the relationships among measured CT indices and between CT indices and PFT values. P values less than .05 were considered statistically significant.

**RESULTS**

**Reproducibility of Tracheal Volume Measurements**

The intra- and interobserver reproducibility of tracheal volume measurements is shown in Table 2. The mean difference did not appreciably deviate from zero, and the limits of agreement were small (Fig 2).
Tracheal Measurements

Table 3 demonstrates the measurements of the tracheal cross-sectional and tracheal volume. The mean cross-sectional area of the upper-trachea decreased from 273.3 mm$^2$ ± 63.7 at inspiration to 236.4 mm$^2$ ± 60.2 at end-expiration, and the mean E/I ratio was 0.87 ± 0.12. Similar observations were found for the lower trachea (273.1 mm$^2$ ± 66.7 at inspiration, 234.4 mm$^2$ ± 62.1 at end-expiration, and E/I ratio of 0.86 ± 0.11). The mean tracheal volume also decreased from 24.6 mL ± 6.8 at inspiration to 19.5 mL ± 6.1 mL at end-expiration, with the mean E/I ratio of 0.79 ± 0.13. Strong, positive correlations ($P < .0001$) were found between measurements of the tracheal cross-sectional area and tracheal volume on both inspiratory and expiratory scans (upper trachea, $r = 0.855$ at inspiration, $r = 0.879$ at expiration; lower trachea, $r = 0.816$ at inspiration, $r = 0.818$ at expiration, respectively). The E/I ratios of tracheal cross-sectional areas also showed strong, positive correlations ($P < .0001$) with the E/I ratios of tracheal volume (upper trachea, $r = 0.841$; lower trachea, $r = 0.853$, respectively).

CT-based Lung Volume

CT-based LV was 5.44 L ± 1.35 at inspiration and 3.83 L ± 1.17 at expiration (Table 3). Inspiratory LV showed a strong, positive correlation with TLC ($r = 0.867$, $P < .0001$) and expiratory LV with RV ($r = 0.815$, $P < .0001$), respectively.

Correlations between Tracheal Volume and CT-based Lung Volume

Table 4 shows correlations between tracheal volume measures and LV measures. Moderate or strong, positive correlations were found between inspiratory tracheal volume and inspiratory LV ($r = 0.661$, $P < .0001$), and between expiratory tracheal volume and expiratory LV ($r = 0.749$, $P < .0001$, Fig 3). Further, the E/I ratio of tracheal volume demonstrated a strong, positive correlation with the E/I ratio of LV ($r = 0.711$, $P < .0001$, Fig 3).

Correlations between Tracheal Volume and Lung Function

Correlations of tracheal volume measurements and PFT results are shown in Table 4. A moderate, negative correlation was found between end-expiratory tracheal volume and FEV$_1$/FVC ($r = -0.445$, $P < .0001$). Also, the E/I ratio of tracheal volume showed moderate or weak, negative correlations with FEV$_1$/FVC ($r = -0.436$, $P < .0001$) and FEV$_1$%...
DISCUSSION

In the current study, we first demonstrate tracheal volumetric measurements and their correlations with LV measurements. In addition to significant correlations between LV and tracheal volume both on inspiratory and end-expiratory scans, collapsibility of the trachea is strongly correlated with collapsibility of the lung. The E/I ratio of the trachea negatively correlates with FEV1/FVC and FEV1 (% predicted), suggesting that higher collapsibility of the trachea indicates less severe airflow limitation or air-trapping in the 85 subjects.

Although tracheal collapse in COPD has been investigated in some studies (11–14,29), it still remains ambiguous as to whether it is directly correlated with lung function. To the best of our knowledge, only a limited number of studies has discussed the relationship between tracheal collapsibility and PFT results (13,14), which leads to the conclusion that high collapsibility of the trachea does not solely indicate compromised lung function. It has also been reported that no significant difference is found in the presence of airway malacia among GOLD stages (13). Furthermore, similar to an early study by Thiriet and colleagues (10), Boiselle and colleagues have recently demonstrated that the highly collapsed trachea (>50% in cross-sectional area) on dynamic-expiratory CT scans, which is concordant with the current diagnostic criteria of TM/TBM, is frequently observed in subjects with normal lung function (9). These results suggest that it still remains difficult to distinguish a severe tracheal collapse in normal subjects from an abnormal collapse in TM/TBM, and that it is useful to understand the mechanism of tracheal collapsibility using some other factors outside the trachea. The current study suggests that the highly collapsed trachea, observed on end-expiratory CT scans, indicates less severe airflow limitation or air-trapping in smokers. These observations can be partially explained by the prediction that LV would be maintained on end-expiratory scans in more severe COPD patients, because of severe air-trapping or expiratory airflow obstruction (15), resulting in smaller changes in intrathoracic pressure and in the tracheal size. However, it has also been acknowledged that smoking, severe emphysema, and chronic bronchitis are contributors to the development of TM/TBM (4). Further, it can be predicted that the trachea can collapse more highly on dynamic expiratory scans in more severe COPD patients, because of severe air-trapping or expiratory airflow obstruction (15), resulting in smaller changes in intrathoracic pressure and in the tracheal size. However, it has also been acknowledged that smoking, severe emphysema, and chronic bronchitis are contributors to the development of TM/TBM (4).

| TABLE 4. Correlations of Tracheal Volume with CT-based Lung Volume and with Lung Function |
|---------------------------------|---------------------------------|---------------------------------|---------------------------------|---------------------------------|
|                                | CT-based Lung Volume            | Lung Function                   |                                |
|                                | Inspiration                     | Expiration                      | E/I Ratio                       | FEV1/FVC (% predicted)          |
| Tracheal volume                |                                |                                |                                |                                |
| Inspiration                    | 0.661*                          | 0.472*                          | −0.126                         | −0.221*                         |
| Expiration                     | 0.677*                          | 0.749*                          | 0.293*                         | −0.445*                         |
| E/I ratio                      | 0.135                           | 0.551*                          | 0.711*                         | −0.436*                         |
are less sensitive in evaluating tracheal collapse than dynamic expiratory scans, particularly in TM/TBM (1,2,4,5). In fact, compared with a study for COPD subjects using dynamic expiratory scans (29), collapsibility of the trachea was much smaller and might have been underestimated in this study. However, based on the fact that end-expiratory scans have been used more frequently and proved to be effective in COPD analysis (15,30,31), we believe that it is still meaningful to demonstrate tracheal collapsibility using end-expiratory scans in general COPD subjects.

Second, inspiratory and end-expiratory scans were obtained without the spirometry-gated technique in our study, which may lead to questioning of whether these scans were truly obtained at subjects’ full inspiration and full expiration. In this study, inspiratory LV was smaller than plethysmographic TLC and expiratory LV larger than RV, which is similar to previous studies (17,18,32,33). These disturbances between CT-based LV and plethysmographic measures can be partially explained by a lack of patient cooperation, the difference of the body position, or the larger effort of breath-holding at expiratory CT scanning than at PFT.

Third, tracheal volume measured in the study requires further discussion. We measured intrathoracic tracheal volume, which was measured from the top of the apex to the carina, suggesting that the apical point would have been influenced by the location and size of the lung in each subject. However, it is known that the intrathoracic part of the trachea behaves differently from the extrathoracic part of the trachea (20). Further, from the perspective of programming automatic measurements, we believe that this apical point is a reasonable and the easiest anatomical location for the standardized method.

Fourth, the number of subjects in the current study was relatively small. This may be one of the reasons that we rarely found subjects with severe tracheal collapse, compared to a large study, which enrolled more than 1000 smokers and found some cases with the highly collapsed trachea using similar end-expiratory CT scans (12).

Fifth, two different scanning protocols were used in this study, which may lead to a questioning of our original CT data and the reliability of measured parameters. Compared with other CT indices, such as MLD or low attenuation area percent, it is predictable that LV or tracheal volume are less sensitive to the differences in scanning protocols, because the upper threshold of ~500 Housfield units is the only point to be influenced by the protocols. We believe therefore that the difference in the protocols did not severely impact the measurements, and that the major observations in the current study were not amplified.

In summary, we first measured tracheal volume and analyzed volumetric measurements of the trachea with lung indices using inspiratory and end-expiratory CT scans. Significant correlations were found between tracheal volume and LV, as well as correlations between collapsibility of the trachea and collapsibility of the lung. Further, higher collapsibility of the trachea did not indicate lower FEV1/FEV1%predicted, lower FEV1/FVC, or higher RV/TLC in this study.

Figure 3. Correlations between measurements of tracheal volume and lung volume. Strong or moderate, positive correlations are found between inspiratory tracheal volume and inspiratory lung volume (a, \( r = 0.661, P < 0.0001 \)), between expiratory tracheal volume and expiratory lung volume (b, \( r = 0.749, P < 0.0001 \)), and between the expiratory/inspiratory (E/I) ratios of tracheal volume and lung volume (c, \( r = 0.711, P < 0.0001 \)).
REFERENCES